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## **Brain-Computer Interface**

Christoph Guger, CEO Guger Technologies OEG g.tec medical engineering GmbH Graz & Linz, Austria

biomedical engineering program





## g.tec – "accelerate your biosignal research"



## company fields

- bio-engineering, medical electronics (bio-electricity)
- developing and offering hard- and software products for biosignal research (single cell activity, EEG, ECoG; muscle cells: ECG, EMG; other tissue: EOG, ...)
- performs user specific adaptations and developments
- mainly based on rapid prototyping environment under MATLAB/Simulink

## company description

- private company, located in Graz and Schiedlberg (Linz), Austria
- inter-disciplinary team (biomedical-, telematics engineers, psychologists)
- customers: universities, university hospitals, R&D departments, industry



#### **Cooperations**

EU IST- Virtual Reality



**Tracking subject responses** in the VE by neuro-physiological measurements: building better VE, therapy applications for patients with anxiety psychosis, ...

- Virtual Environments and Computer Graphics, UPC, Barcelona Mel Slater, Chris Groenegress
- University of Technology Graz, Austria Robert Leeb, Gert Pfurtscheller
- Insituto de Neurociencias, UMH, Alicante, Spain Mavi Sanchez-Vives
- UPF Barcelona Paul Verschure











### **Range of Products**





## Content

- a) What is a BCI?
- b) Applications
- c) Components of a BCI
- d) Physiological background
- e) ERD/ERS
- f) Slow cortical potentials
- g) SSVEPs
- h) P300
- i) Spelling with the BCI
- j) Smart home control





## **Brain Computer Interface**



## **III)** Closed loop Applications:

## **Brain-Computer-Interface (BCI) in VR**





... establishes the only communication channel without using any muscle activity ...

a BCI transforms EEG signals into control signals

- HCI Human Computer Interface
- DBI Direct Brain Interface (University of Michigan)
- TTD Thought Translation Device (University of Tübingen)



## Applications of a BCI in patients



- patients with amyotrophic lateral sclerosis (ALS)
- locked-In Syndrome (LIS) to communicate
- patients with **amputations** to control a robotic limb
- patients with **spinal cord lesions** to control a FES device or a wheelchair
- gaming
- composing music
- walking through VE, controlling VE









## Applications of a BCI in subjects/patients



#### Potential users worldwide

Cerebral palsy Brainstem stroke Other stroke Spinal cord injury Postpolio syndrome Amyotrophic lateral sclerosis Multiple sclerosis Muscular dystrophy Guillain-Barre syndrome

- -16,000,000
- -10,000,000
- -60,000,000
- -5,000,000
- -7,000,000
- 400,000/3,000,000
- -2,000,000
- 1,000,000
- 70,000



## **Evolution of BCI research**



- 1995 ~ 5 labs active in BCI research, first demonstrations
- 2005 > 70 laboratories active all over the world
- 2007 > 120 laboratories involved in BCI research



#### **Growth of BCI publications in peer-Reviewed Papers**



## **Evolution of BCI research**



• "BCI Activity Map" > 120 sites



Adapted from Schalk et al.



## **Evolution of BCI research**



Case Studies from



Case studies 2007



# Changes of brain electrical activity and mental strategies



- Slow cortical potentials (anticipation tasks) DC-derivation, artifact problem, difficult strategy, feedback method
- Steady-State Evoked potentials (SSVEP, SSSEP) Flickering light with specific freugency

## Event-related, non-phase-locked changes of oscillatory activity ERD/ERS (motor imagery tasks)

Changes of mu-rhythm, alpha activity and beta activity over sensorimotor areas, imagination of hand- ,foot-, tongue- movements

## - Evoked potentials (focus on attention task)

Thalamic gating, various methods of stimulation (visual, tactile, electrical, auditory, ...), P300



## **Measurement of brain signals**

Multi-channel analysis system with derivations simultaneously and also directly in the brain

Electroencephalogram
non-invasive

bad spatial resolution

Electrocorticogram

direktly measured on brain's surface good spatial resolution

 Micro-electrode arrays implanted into the brain best signal quality









## **Excursus: Measuring brain activity**



#### Electroencephalogram (EEG)

small electrodes (#1 - #256) attached to the surface of the scalp place electrodes at certain predefined positions according to the "international 10/20 system"

EEG amplitudes: **5 – 100 uV** EEG frequencies: **1 – 40 Hz** 

EEG: non-stationary time signal varies greatly between subjects low signal-to-noise ratio

- spatio-temporal patterns
- non-invasive







## **Excursus: Measuring brain activity**



#### Electro-corticogram (ECoG)

4 mm diameter

~ 100 electrodes

EEG amplitudes: **0.5 mV** EEG frequencies: **1 – 100 Hz** 



modified from University of Michigan

- resolution considerably better than EEG
- provides opportunity for multi-channel control
- more direct correlation to activity

#### invasive

limited study opportunities



modified from University of Michigan





## **Steps in BCI development**



Step 1: Selection of parameter estimation and classification algorithms

Step 2: Implementation of the algorithms

Step 3: Off-line simulation

Step 4: Connection to the real world

Step 5: Real-time code generation

Step 6: Real-time tests



## Why Rapid Prototyping?











## **Closed loop system g.BClsys**





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MathWorks

Partner



## Requirements to successfully run BCI experiments





## **Hardware Development**

EEG, ECoG, EMG, EOG, ECG amplifiers 1-128 channels

A. USB based biosignal amplifier 16 integrated 24 Bit ADCs Floating point DSP re-referencing oversampling (~20000 times) bandpass and notch filtering

## B. Mobile device

2-4 AA batteries1 integrated 16 Bit ADCserial/USB interface1 week operation timeTCP/IP remote control

C. Stand-alone device analog output combine it to DAQ board (e.g. NI) resolution sampling frequency PCI or PCMCIA board









## **Software Programming Environment**



DCI C

Bandpowe

andnome

Brain Computer Interface with g.MOBIIat

- 0 ×

A. C++ Application Program Interface amplifier

## B. MATLAB API

- integrate amplifiers into MA
- access to all toolboxes (Sig
- access to user written M-file

## C. Simulink Highspeed on-line Pro

- amplifier device driver block under Simulink
- copy the block into Simulink model and connect the signal processing (S-functions) and paradigm blocks (MATLAB code)

Gain2

 just exchange the amplifier device driver and work with the same signal processing blocks

#### All three options give full access to hardware

- bandpass, notch settings
- sampling frequency
- impedance check
- data buffer
- ...



(I)

## Selection of parameter estimation algorithms



## Non adaptive estimation: Band power (optimal frequency bands) KALCHER et al. 1993

AR parameters

PFURTSCHELLER et al.1997 WOLPAW 1997

Hjorth parameters

GUGER 1997, OBERMAIER et al. 1999 Common Spatial Patterns (CSP) MÜLLER - GERKING et al. 1999, RAMOSER 2000 GUGER 2000

### (II) Adaptive estimation

AAR parameters (RLS algorithm) SCHLÖGL





## Selection of classification algorithms



(I) Neural networks (>= 2 classes) LVQ, DSLVQ

> FLOTZINGER et al. 1994 PREGENZER and PFURTSCHELLER 1999

(II) Linear discriminant (2 classes) ✓ signed distance function

> PFURTSCHELLER et al. 1998 LUGGER et al. 1998

(III) Hidden Markov Models (>=2classes) OBERMAIER et al. 2001

(IV) Support-Vector Machines MÜLLER





- library for standard neuro- and psycho-physiological paradigms
- accurate timing for visual, auditory and tactile stimulation
- MATLAB based paradigm parser for easy development of user-specific experiments
- logging of subject responses and real-time biofeedback to the subject/patient
- create easily test batteries for cognitive tasks (human intelligence and neural efficiency) and motor tasks (rehabilitation for stroke, epilepsy, Parkinson's disease)
- simulate traffic flow or flight control scenes to investigate the workload of pilots www.gtec.at













## Requirements for high quality EEG recordings and BCI applications



- The lab: shielding, light, monitor position, chair, silence
- Technical aspects: amplifier placement, electrode leads, type of electrode/cap, impedance, ...
- The artifact problem: amplifier, electrodes, physiological artifacts, systematic artifacts
- Instruction of the subject: fixation cross, muscle relax, eye-blinks, duration of runs, breaks, motivation



## How can the computer read your thoughts?



Produce unique brain activity patterns

Think about a hand/foot movements

Concentrate on an event - flashing letter



High-end and robust brain signal amplifier







## Signal processing & Pattern recognition







# Changes of brain electrical activity and mental strategies



- Slow cortical potentials (anticipation tasks) DC-derivation, artifact problem, difficult strategy, feedback method
- Steady state evoked potentials (focus of attention task) Thalamic gating, various methods of stimulation (visual, tactile, electrical, auditory, ...)
- Phase-locked potentials, readiness potentials, motor potentials (motor tasks)
  Template matching, spatial distribution, large number of electrodes, ECoG electrode grid
- Event-related, non-phase-locked changes of oscillatory activity ERD/ERS (motor imagery tasks)
  Changes of mu-rhythm, alpha activity and beta activity over sensorimotor areas, Imageries of hand- ,foot-, tongue- movements


## **Communication for the 'locked-in'**



ALS patient in Germany using a BCI system for communication Birbaumer, Kübler, Hinterberger,... Tübingen







## Changes of brain electrical activity and mental strategies



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# Steady-State Visual Evoked Potentials (SSVEP)

| Frequency of stimulation |  |
|--------------------------|--|
| 0 2 Hz                   |  |
| 3 5 Hz                   |  |
| 6 24 Hz                  |  |

Brain response

transient (single) VEP

undefined response

**SSVEP** 



# Steady-State Visual Evoked Potentials (SSVEP)

7 Hz





## **Steady-State Visual Evoked Potentials**



7 Hz





# Steady-State Visual Evoked Potentials (SSVEP)





## **Steady-State Visual Evoked Potentials**



Fig. 1. Amplitude spectra of SSVEPs induced by 6.83- (thick) and 7.03-Hz (thin) visual stimulation.



# Steady-State Visual Evoked Potentials (SSVEP)



## up to 48 different frequencies possible!



#### **ERD/ERS BCI**



## Changes of brain electrical activity and mental strategies



- Slow cortical potentials (anticipation tasks) DC-derivation, artifact problem, difficult strategy, feedback method
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## The ``Motor Imagery Task``



Event-related desynchronization (ERD) and sychronization (ERS) over sensory-motor areas occur for ...

... planning of movements

... execution of movements

... imagination of movements

... passive movements

(... observation of movements)

#### Physiological Background – why does it work g.te GUGER TECHNOLOGIES Left hand Right hand movement movement $\circ_{\circ}$ ० RIGHT Cz C4 0 Nasion 0 0 Inion REF

Imagination of hand movement causes an ERD which is used to classify the side of movement. The desynchronization occurs in motor and related areas of the brain. Therefore, for analyzing and classifying ERD-patterns the electrodes must be placed close to sensorimotor areas.





## C3 The ``Finger Movement Task``

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## **Oscillatory EEG Activity (example)**



| Anna and Anna and an anna anna an anna an anna an anna an an  | 20 μV            |
|---|------------------|
| APPAPara MANAMANA ANA ANA ANA ANA ANA ANA ANA AN  | <u>1 s</u>       |
| WARMAN MANAMAN MANAMANA MANAMANA MANAMANA MANAMANA  | C3               |
| Monoral Marken and a second and a   | right<br>index   |
| MAYARAMAMAMAMANA MARAMANA AND A A A A A A A A A A A A A A A A   | finger           |
| MANNAMANAMANAMANAMANAMANAMANAMANAMANAMA   | motor<br>imagery |
| MAN management and a second and a   | inagory          |
| Marmond Mar and a second and a s |                  |
| And any after and an and a second a second and a second a secon  |                  |
| WWWWWWWWWWWWWWWWWWWWWWWWWWWWWWWWWWWWWW  | ŝ.               |
| motor imagery onset   | w.gtec.at        |

## **Oscillatory EEG Activity (example)**

unional maraka in any Marka and prover his and Mary in a far have a some in the marka in the providence in the marka water and a second and the second se - How was a war of the second stand and the second stand and the second stand and the second man and a second a man and the second of the second of the second man manual and a second way was a second and a mananismum mananismum mananismum and a stand with a strain and the second strain and the second strain and the second s man man and a second a second a second and the seco -----man and a second a in a second and the second of - in property was a property of the second s man marine so man make a second with the second second with the market and the second se monorman and the second and the seco minimum and a second ware more many fill the many and the second mounter and mounter and the second second second second and the second s annanger and a second and the second and a second as -----20 µV 1 s # 62, Ch 31, Cz, LAR feedback beep cue





#### Which type of "thought" should be used?





"specific" activation of the hand representation area



#### Somatotopic organisation of the motor cortex







#### **Event-related-desynchronisation/synchronization**







### **Time- frequency mapping of ERD / ERS**

ERD/ERS map for electrode C3, right index finger movement (significant values, p<.05)





![](_page_59_Figure_1.jpeg)

![](_page_59_Picture_2.jpeg)

![](_page_59_Picture_3.jpeg)

Left hand

![](_page_59_Picture_5.jpeg)

Right hand **motor imagery** 

![](_page_59_Picture_7.jpeg)

Foot

![](_page_60_Picture_0.jpeg)

#### **Off-line simulation - Paradigm**

![](_page_60_Picture_2.jpeg)

![](_page_60_Figure_3.jpeg)

![](_page_61_Picture_0.jpeg)

### **Training BCI Control**

![](_page_61_Picture_2.jpeg)

![](_page_61_Picture_3.jpeg)

| Training phase                          |                              |  |  |  |  |
|---|------------------------------|--|--|--|--|
| <b>- X - X - X - X</b>                  |                              |  |  |  |  |
| ←                                       | $\rightarrow$                |  |  |  |  |
| E C C C C C C C C C C C C C C C C C C C |                              |  |  |  |  |
| eedback / BCI application phase         |                              |  |  |  |  |
| eedback / E                             | <b>BCI</b> application phase |  |  |  |  |
|   | BCI application phase        |  |  |  |  |
|   | BCI application phase        |  |  |  |  |

![](_page_62_Picture_0.jpeg)

## Connection to real world – Imagination with continuous feedback

![](_page_62_Picture_2.jpeg)

![](_page_62_Figure_3.jpeg)

![](_page_63_Picture_0.jpeg)

### g.USBamp Simulink Highspeed on-line Processing

- amplifier device driver block reads data into Simulink in real-time
- blocks for signal visualization and data storage
- feature extraction with bandpower algorithm implemented as S-function in C
- on-line linear discriminant analysis
- paradigm implemented as S-function with MATLAB code

![](_page_63_Figure_7.jpeg)

![](_page_63_Picture_8.jpeg)

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![](_page_64_Picture_0.jpeg)

#### **Training Results**

![](_page_64_Picture_2.jpeg)

Classification Results, T.S., Age: 22, Mai - September, T1-T62

![](_page_64_Figure_4.jpeg)

![](_page_65_Picture_0.jpeg)

![](_page_66_Picture_0.jpeg)

### How many people can control a BCI?

- BCI system at exhibition about bio-technology in Graz (6 months duration)
- data of all 99 subjects (first 2 month)
- 1 run without feedback
- next run with feedback

• 2 bipolar derivations analyzed with adaptive autoregressive parameters or bandpower of predefined frequency bands

| Classification<br>Accuracy in % | RLS<br>Percentage of<br>Runs<br>(N=76) | BP<br>Percentage of<br>Runs<br>(N=117) | RLS+BP<br>Percentage of<br>Runs<br>(N=193) |
|---------------------------------|--|--|--|
| 90-100                          | 6.6                                    | 6.0                                    | 6.2  |
| 80-89                           | 10.5                                   | 14.5                                   | 13.0                                       |
| 70-79                           | 30.3                                   | 33.3                                   | 32.1                                       |
| 60-69                           | 40.8                                   | 42.7                                   | 42.0                                       |
| 50-59                           | 11.8                                   | 3.4                                    | 6.7  |
|                                 | 100                                    | 100                                    | 100  |

![](_page_66_Picture_8.jpeg)

![](_page_67_Picture_0.jpeg)

#### **Position reconstruction with place cells**

![](_page_67_Picture_2.jpeg)

Place cells are located in the hippocampus

Place cells fire only at specific positions

The action potentials are measured with tetrodes inserted into the animal brain

**Recordings performed with rats** 

cell 1

cell 2

![](_page_67_Picture_9.jpeg)

![](_page_67_Picture_10.jpeg)

![](_page_68_Figure_0.jpeg)

![](_page_69_Picture_0.jpeg)

#### Accuracy of position recognition

![](_page_69_Picture_2.jpeg)

![](_page_69_Figure_3.jpeg)

![](_page_70_Picture_0.jpeg)

Live Experiment: I) P300 based speller

![](_page_70_Picture_2.jpeg)

![](_page_71_Picture_0.jpeg)

## Changes of brain electrical activity and mental strategies

![](_page_71_Picture_2.jpeg)

- Slow cortical potentials (anticipation tasks) DC-derivation, artifact problem, difficult strategy, feedback method
- **Evoked potentials (focus of attention task)** Thalamic gating, various methods of stimulation (visual, tactile, electrical, auditory, ...), P300
- Phase-locked potentials, readiness potentials, motor potentials (motor tasks)
   Template matching, spatial distribution, large number of electrodes, ECoG electrode grid
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   Changes of mu-rhythm, alpha activity and beta activity over sensorimotor areaswww.gtec.at Imageries of hand- ,foot-, tongue- movements


## Physiological background



## P300 - Evoked Response Potential (ERP)

- is obtained from EEG's (spontaneous brain activity) by averaging techniques

- is generated by a specific stimulus, i.e. visual or auditory cue.

- elicited commonly in an "oddball" paradigm when a subject detects an occasional "target" stimulus in a regular train of standard stimuli.

- only occurs if the subject is actively engaged in the task of detecting the targets.

Its amplitude varies with the improbability of the targets. Its latency varies with the difficulty of discriminating the target stimulus from the standard stimuli (Picton 1992, discovered by Sutton et al. 1965)





## P 300 Visually Evoked Potentials



Cognitive relevance: What generates a large P 300 component?

- I can detect the target stimulus out of a number of non-targets

- I draw more attention to the target stimulus than to the others
- I can recognize the target stimulus
- I am waiting for the target stimulus to appear
- The target stimulus contains more information than the non-target
- The target has any other property that makes it unique



concentrate on "W"

Individual character intensifies for 60ms with 10ms between each intensification

| Α | В | С | D | Е | F |
|---|---|---|---|---|---|
| G | н | I | J | К | L |
| Μ | Ν | Ο | Р | Q | R |
| S | т | U | V | W | X |
| Y | Ζ | 0 | 1 | 2 | 3 |
| 4 | 5 | 6 | 7 | 8 | 9 |







| Α | В | С | D | Е | F |
|---|---|---|---|---|---|
| G | н |   | J | K | L |
| М | Ν | 0 | Ρ | Q | R |
| S | Т | U | V | W | Х |
| Y | Ζ | 0 | 1 | 2 | 3 |
| 4 | 5 | 6 | 7 | 8 | 9 |





| A | В | С | D | Е | F |  |
|---|---|---|---|---|---|--|
| G | Н |   | J | K | L |  |
| Μ | Ν | 0 | Ρ | Q | R |  |
| S | т | U | V | W | Х |  |
| Y | Z | 0 | 1 | 2 | 3 |  |
| 4 | 5 | 6 | 7 | 8 | 9 |  |
| 4 | 5 | 6 | 7 | 8 | 9 |  |





| Α | В | С | D | Е | F |
|---|---|---|---|---|---|
| G | н |   | J | К | L |
| Μ | Ν | 0 | Ρ | Q | R |
| S | Т | U | V | W | X |
| Y | Ζ | 0 | 1 | 2 | 3 |
| 4 | 5 | 6 | 7 | 8 | 9 |





| Α | В                     | С            | D                  | E                        | F   |
|---|-----------------------|--------------|--------------------|--------------------------|---|
| G | н                     |              | J                  | K                        | L   |
| Μ | N                     | 0            | Р                  | Q                        | R   |
| S | т                     | U            | V                  | W                        | X   |
| Y | Z                     | 0            | 1                  | 2                        | 3   |
| 4 | 5                     | 6            | 7                  | 8                        | 9   |
|   | A<br>G<br>M<br>S<br>Y | ABGHMNSTYZ45 | ABCGHIMNOSTUYZO456 | ABCDGHIJMNOPSTUVYZO14567 | A B C D E   G H I J K   M N O P Q   S T U V W   Y Z O 1 2   4 5 6 7 8 |



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0.7



#### Mount electrodes





International 10/20 system. The distances between Inion-Nasion and the left and rigth preauricular points are the basis for the location of all electrode positions.



## **Placement of the cap**







#### P300 BCI? Study Design



5 subjects, 8 EEG channels recorded Fz, Cz, P3, Pz, P4, PO7, Oz, PO8 Referenced to right mastoid, grounded to the forehead Data recorded with g.USBamp

Fa = 256 Hz, bandpass 0.1 – 30 Hz 1st training run -> 5 letters Application runs -> up to 42 letters

"Spelling Device" Application

Single character flash experiment

 $\rightarrow$  Total of ~ 45 min incl. electrode montage and instruction of the subject





#### **Feature Extraction**

Event related data triggering: 100ms pre-stimulus, 700ms post-stimulus Baseline correction was performed for pre-stimulus interval Downsampling (15 features/channel \* 8 channel) Data segments were concatenated by channel

Assume 5 flashes were selected for training, 3 letter word e.g. BCI single character mode: 36\*5 = 180 flashes \* 3 repetitions 540 trials, 15 target trials, 525 non target trials

Feature matrix 180\*120 -> LDA







#### Accuracy depends on letters used for classifier training



#### **3 training characters**



#### 42 training characters



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#### Grand Average P300 responses



EP reaches about 5-6  $\mu$ V, 350 ms after stimulus No difference over time -> stable





#### **Transfer rates calculation**

The bit rate R in bits/min is given by

 $\mathbf{R} = \mathbf{B} \cdot \mathbf{M}$ 

$$\mathbf{B} = \log_2 \mathbf{N} + \mathbf{P} \cdot \log_2 \mathbf{P} + (1 - \mathbf{P}) \cdot \log_2 \left[ \frac{(1 - \mathbf{P})}{(\mathbf{N} - 1)} \right]$$

where N is the number of possible selections, P is the accuracy probability and M is the average number of decisions per minute **Average transfer rates of all subjects** 





## Neurofeedback Applications: P300 Speller, row/column flash g.USBamp, g.MOBIIab, High-Speedonline Processing, g.RTanalyze, different sensors



Time [1:24]





#### Live Experiment: II) Smart Home Control XVR and BCI



## P300 for smart home control





Designed by Chris Groenegress, Mel Slater



#### P300 for smart home control





Designed by Chris Groenegress, Mel Slater

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## P300 for smart home control





Designed by Chris Groenegress, Mel Slater



## **Control matrix for smart home**







## **Goto specific position – The Beamer**







#### Discussion



The performance of a BCI system can be measured in terms of:

**Decision speed** (how many seconds are required for one decision?) 1-10 seconds for one decision with P300 same for osciallatory, SSVEP and slow waves

## BUT

#### Degrees of freedom (how many classes can be selected?)

motor imagery task: max. 3 – 4 classes possible slow cortical shift: continuous feedback for one dimension (up-down) steady-state evoked potentials: up to 12 keys (phone keyboard) P300-spelling: e.g. 36 letters (6 x 6 matrix) or more

#### P300 allows better control of smart home



## Discussion



External visual stimuli P300 need flashing characters -> it is not the thought of the subject

SSVEP – needs flickering light

Motor imagery BCI detect left/right hand movement, but there is also a trigger signal required that tells the subject when to think about the movement

Slow waves - need timing information

Accuracy (how many decisions are correct?) Accuracy of 95 – 100 % possible for most subjects

#### Next steps:

Integration of the P300 BCI into highly immersive environment as a new way of communication



# **Some General Remarks:**

- The Accuracy-vs.-Speed Problem (Transfer rate bit/min)
- Adaptive Algorithms: 2 Learning Systems !!!
- `State ot the Art`: from Research to Practical Use
- Acceptance & Usability: Evaluation by Patients and Caregivers
- Assets and Drawbacks of BCI compared to other Interfaces



# **Potential for Further Improvement**

| Parameter<br>Extraction<br>Methods                   | Classification<br>Algorithms     | Improved<br>Sensors and<br>Electrodes                    |  |
|--|----------------------------------|--|--|
| Implanted Sensors<br>with Wireless<br>Transmission   | Combination of different Methods | New Applications   |  |
| Online-Statistics<br>for Optimized<br>Decision Speed | Artifact<br>Reduction<br>Methods | Assistive Systems:<br>Text Completion,<br>Speech output, |  |

# **Biomedical Engineering Lectures in PDF format**





Tutorial contain theory and tasks (measurements, analysis,...) Solutions in a second manual

Very useful in education and to get into the field







BCI WORKSHOP Graz, Austria g.tec BCI Workshop TU Graz BCI Conference September 2008 150 people

BCI Workshop @ Neuroscience, Washington DC, USA November 2008

We have open positions for PHD students and master students.





http://www.presenccia.org

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